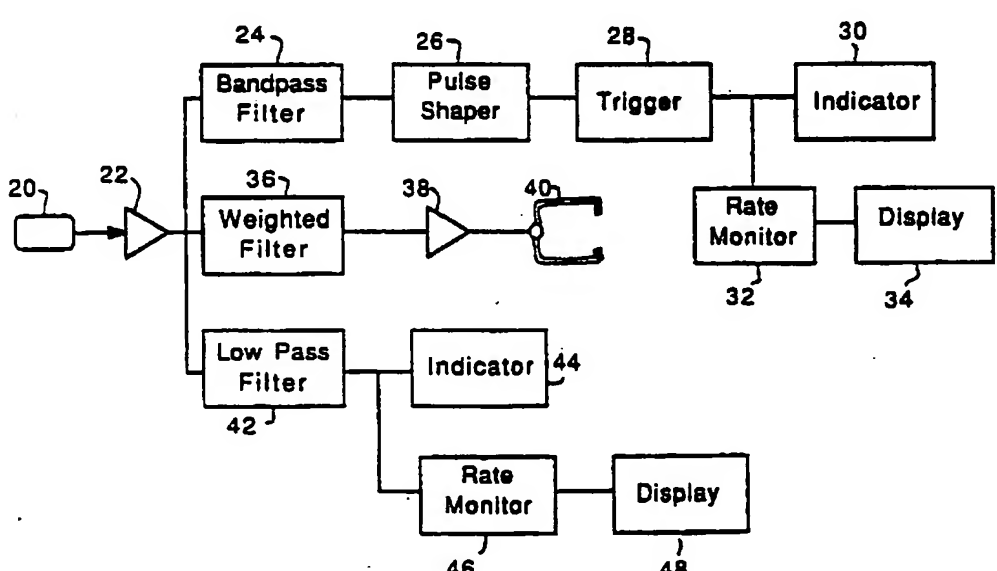




## INTERNATIONAL APPLICATION PUBLISHED UNDER THE PATENT COOPERATION TREATY (PCT)

<p>(51) International Patent Classification <sup>5</sup> : <b>A61B 5/0255</b></p>	<p><b>A1</b></p>	<p>(11) International Publication Number: <b>WO 92/09232</b> (43) International Publication Date: 11 June 1992 (11.06.92)</p>
<p>(21) International Application Number: PCT/US91/08905 (22) International Filing Date: 26 November 1991 (26.11.91) (30) Priority data: 618,297 27 November 1990 (27.11.90) US (71)(72) Applicant and Inventor: PEEL, Harry, Herbert, III [US/US]; 3006 Quakertown, San Antonio, TX 78230 (US). (74) Agent: HAMILTON, Gary, W.; Pravel, Gambrell, Hewitt, Kimball &amp; Krieger, 1177 West Loop South, Suite 1010, Houston, TX 77027 (US). (81) Designated States: AT (European patent), AU, BE (European patent), CA, CH (European patent), DE (European patent), DK (European patent), ES (European patent), FR (European patent), GB (European patent), GR (European patent), IT (European patent), JP, LU (European patent), NL (European patent), SE (European patent).</p>		<p>Published With international search report.</p>
<p>(54) Title: VITAL LIFE SIGN DETECTOR</p>  <p>(57) Abstract</p> <p>A vital life sign detector which can be used to determine heart and respiration activity in an individual wearing bulky clothing, such as chemical warfare protective clothing. A detector (20), such as an accelerometer or geophone, detects chest wall vibrations of an individual and produces an output signal (22) in response thereto. The output signal is processed to determine the existence of cardiac and respiratory activity. The output signal can be further processed to calculate the heart rate and respiration rate of the individual. The system produces a visual (34) or audio signal (40) which allows medical personnel to determine quickly whether the individual is alive.</p>		

**FOR THE PURPOSES OF INFORMATION ONLY**

Codes used to identify States party to the PCT on the front pages of pamphlets publishing international applications under the PCT.

AT	Austria	ES	Spain	MG	Madagascar
AU	Australia	FI	Finland	ML	Mali
BB	Barbados	FR	France	MN	Mongolia
BE	Belgium	GA	Gabon	MR	Mauritania
BF	Burkina Faso	GB	United Kingdom	MW	Malawi
BG	Bulgaria	GN	Guinea	NL	Netherlands
BJ	Benin	GR	Greece	NO	Norway
BR	Brazil	HU	Hungary	PL	Poland
CA	Canada	IT	Italy	RO	Romania
CF	Central African Republic	JP	Japan	SD	Sudan
CG	Congo	KP	Democratic People's Republic of Korea	SE	Sweden
CH	Switzerland			SN	Senegal
CI	Côte d'Ivoire	KR	Republic of Korea	SU <sup>+</sup>	Soviet Union
CM	Cameroon	LI	Liechtenstein	TD	Chad
CS	Czechoslovakia	LK	Sri Lanka	TG	Togo
DE <sup>+</sup>	Germany	LU	Luxembourg	US	United States of America
DK	Denmark	MC	Monaco		

<sup>+</sup> Any designation of "SU" has effect in the Russian Federation. It is not yet known whether any such designation has effect in other States of the former Soviet Union.

## VITAL LIFE SIGN DETECTOR

1

2 **Field of**  
3 **the invention**

4       The present invention relates generally to systems for detecting vital life signs in  
5 individuals. More specifically, the present invention provides a method and apparatus for  
6 detecting vital life signs, such as heart rate and respiration, in an individual wearing heavy  
7 garments or other covering. An example of such an individual would be a soldier  
8 wearing arctic clothing or chemical warfare protective gear.

9 **Background of**  
10 **the invention**

11       The first step in a medical emergency is to determine whether the heart is beating  
12 and breathing is present. The heartbeat is classically found by palpating the pulse in the  
13 wrist, neck, or ankle, or by listening to the chest with a stethoscope or ear. Breathing is  
14 typically detected by observing motion of the chest and abdomen or sensing airflow  
15 through the nose and mouth.

16       Situations occur, particularly in wartime, in which it is not possible for a human to  
17 sensorially detect the pulse or breathing. This is particularly true during arctic or  
18 chemical warfare where the casualty and the medical personnel may be completely  
19 encased in heavy clothing and may be wearing heavy gloves or masks. Blood loss,  
20 shock, and trauma may also reduce the intensity of the pulse and respiration which make  
21 sensory detection of vital life signs difficult and time consuming.

22       In situations where large numbers of casualties are present, it is important that care

2 determining the presence of a pulse and breathing is, therefore, a central issue in casualty  
3 management.

4 The prior art has heretofore failed to provide a system for quickly detecting vital life  
5 signs in individuals, such as wartime casualties, who are wearing bulky protective  
6 clothing. The vital life sign detector of the present invention, described in greater detail  
7 below, fulfills this need.

## 2 the invention

3 The vital life sign detector of the present invention overcomes the difficulties of the  
4 prior art by providing a system which can be used to determine heart and respiration  
5 activity in an individual wearing bulky protective coating. In the preferred embodiment  
6 of the invention, a detector, such as an accelerometer or geophone, detects chest wall  
7 vibrations of an individual and produces an output signal in response thereto. The output  
8 signal is processed to determine the existence of cardiac and respiratory activity. The  
9 output signal can be further processed to calculate the heart rate and respiration rate of  
10 the individual. Numerous types of transducers can be used to detect the chest wall  
11 vibrations, including piezoelectric, electromagnetic and resistive transducers.

12 The system of the present invention is contained in a housing which fits comfortably  
13 in the gloved hand of medical personnel and requires little dexterity to activate. The  
14 housing also has dimensions which allow it to be stable when at rest on the individual,  
15 even when the chest surface is at large angles relative to horizontal. The total mass of  
16 the device is sufficient to hold the detector effectively stationary relative to the body of  
17 the patient. The bottom surface of the housing is covered with a nonslip coating to  
18 prevent sliding off the chest.

## 2 of the Drawings

3 FIG. 1 is an illustration of the vital life sign detector of the present invention placed  
4 on an individual.

5 FIG. 2 is a schematic illustration of the signal processing electronics employed in  
6 the vital life sign detector of the present invention.

7 FIG. 3a is a graphical representation of an ECG signal produced by an individual.

8 FIG. 3b is a graphical representation of the output signal of the motion detector  
9 employed in the present invention.

## 2 the Preferred Embodiment

3 FIG. 1 is an illustration of the vital life sign detector of the present invention placed  
4 on the chest of an immobilized individual 12. The detector 10 is provided with an  
5 appropriate display to allow the medical aid personnel 14 to quickly determine whether  
6 the individual 12 is alive. The beating of the heart and breathing produce movements and  
7 accelerations of the individual's body due to changes in organ volume and momentum  
8 transfers. These accelerations and movements can be used to provide an indication of  
9 cardiac output and respiratory volume changes. The movements range from very low  
10 frequencies (respiration: 0.1 to 0.5 Hz; heart rate: 0.5 to 4 Hz) to relatively high  
11 frequencies (breath sounds: 100 to 2000 Hz; heart sounds and bruits: 40 to 1000 Hz).  
12 These movements and vibrations normally can be detected with the finger or with the aid  
13 of a stethoscope applied to the bare skin. However, when clothing or other coupling  
14 materials are introduced between the skin and human sensor, the vibrations and sounds  
15 are filtered with the high frequency components that are normally sensorially detectable  
16 being filtered out. It has been observed by the inventor, however, that the low frequency  
17 components are attenuated to a far lesser extent and can be sensed with low frequency  
18 acceleration measurement devices. The system of the present invention utilizes these low  
19 frequency signals to provide an indication of the existence of vital life signs.

20 In summary, the vital life sign detector is a small device which, when placed upon  
21 a subject, will detect the mechanical vibrations associated with respiratory and heart  
22 movement. Typically, the device is placed on the chest of the supine casualty. The  
23 medical aid provider removes his hand and observes the face of the device. A display

2 A second display indicates respiratory motion and displays the respiration rate.

3 As shown schematically in FIG. 2, the chest wall vibrations produced by cardiac and  
4 respiratory motions are detected with one or more motion detectors 20, such as an  
5 accelerometer or geophone. The motion detectors 20 can use any of a number of  
6 transducers, including, but not limited to, piezoelectric, resistive, or electromagnetic. An  
7 example of the typical output signal from the motion detector 20 is illustrated in FIG. 3b.  
8 The ECG signal is shown in FIG. 3a for reference. It should be noted that there are two  
9 pulses associated with each heart beat. These pulses correspond to the onsets of systole  
10 and diastole and are synchronous with the first and second heart sounds.

11 The signal from the motion detector 20 is first amplified in an appropriate amplifier  
12 22 and then conditioned in several ways. First, for heart rate, the signal is processed by  
13 an analog or digital bandpass filter 24 having a pass band from about 0.5 to about 300  
14 Hz. The transient oscillations are converted and smoothed into a pulse by a pulse shaper  
15 circuit 26. The shaped pulse signal is then fed to a level sensitive, timed, one shot trigger  
16 28 which is held on for approximately 300 msec before resetting. The lock-on time is  
17 consistent with the ejection time of the heart. This time lock-on is to prevent double  
18 triggering by the second pulse. The timed pulse is then used to turn on the front panel  
19 pulse indicator 30 to provide an indication of the existence of cardiac activity. The timed  
20 pulse is also fed to a rate computation means 32, which can utilize analog, digital or  
21 software rate computing techniques, known in the art, to calculate heart rate. The  
22 calculated heart rate is displayed on a front panel display 34.



2 to provide a pseudo heart sound output for the user to hear. To provide this signal, the  
3 transducer signal is passed through a weighted band pass filter 36 which has a transfer  
4 function equivalent to that of a stethoscope. This filtered signal is then fed to a suitable  
5 power amplifier 38 which is connected to an earphone 40. In the preferred embodiment  
6 of the invention, the earphone is mounted in a stethoscope yoke to facilitate use.

7 The output signal of the motion detector 20 is also provided to a third channel which  
8 is used to determine the existence of respiration in the individual by one of several  
9 methods. In one method, the detector signal is processed in an extremely low bandpass  
10 filter 42. The high frequency cutoff of the filter 42 is approximately five Hz. The overall  
11 detector and filter low frequency cutoff should be 0.05 Hz or less. It is preferable that  
12 the low frequency cutoff be defined by the detector rather than the subsequent  
13 electronics. High pass filtering should not be used to avoid long settling times resulting  
14 from any large artifacts introduced into the signal.

15 Another suitable method for detecting respiratory movements from the detector  
16 signal is to measure the beat-to-beat changes in the intensity of the pulses. The intensity  
17 of the pulses are due, in part, to the compliance of the chest within which the heart is  
18 beating. The compliance of the chest is dependent upon the volume of air contained  
19 within the lungs and the muscle tension of the chest muscle, both of which will change  
20 during the course of respiration. The cyclical compliance variations during breathing  
21 produce the cyclical variations in the detected pulse amplitudes.

22 The low frequency components produced by filtering methods or the variations in

2 Either signal is also fed to a rate computation means which can utilize analog, digital, or  
3 software rate computing techniques, known in the art, to calculate respiration rate.

4 Careful attention to the housing design is required for the detector to operate  
5 properly to detect heart beat and respiration through garments. The device should fit  
6 comfortably in the gloved hand of medical personnel and should require little dexterity  
7 to activate. The housing should have dimensions which allow it to be stable when at rest  
8 on the individual, even when the chest surface is at large angles relative to horizontal.  
9 The total mass of the device must be sufficient to hold the detector effectively stationary  
10 relative to the body of the patient. A rectangular box of 4" x 3" x 1" having a weight of  
11 one pound has been found to be a satisfactory upper limit. The bottom surface of the  
12 housing should also be covered with a nonslip coating to prevent sliding off the chest.  
13 The displays should be large and designed to be easily read especially from low angles  
14 relative to the display. Finally, the device package should be sealed against contaminants  
15 since, as an emergency device, it will be used in hostile environments.

16 Although the vital life sign detector of the present invention has been described in  
17 connection with the preferred embodiment, it is not intended to be limited to the specific  
18 form set forth herein, but on the contrary, it is intended to cover such modifications,  
19 alternatives, and equivalents as can be reasonably included within the spirit and scope of  
20 the invention as defined by the appended claims.

- 2 1. A system for detecting vital life signs in an individual, comprising:  
3 means for detecting vibrations in the chest wall of an individual and for  
4 producing an output signal in response thereto, even when said  
5 individual is wearing bulky clothing;  
6 means for correlating said output signal with vital life signs of said  
7 individual.

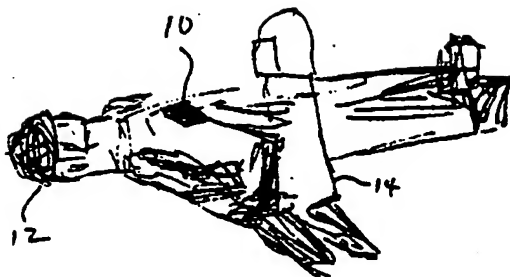
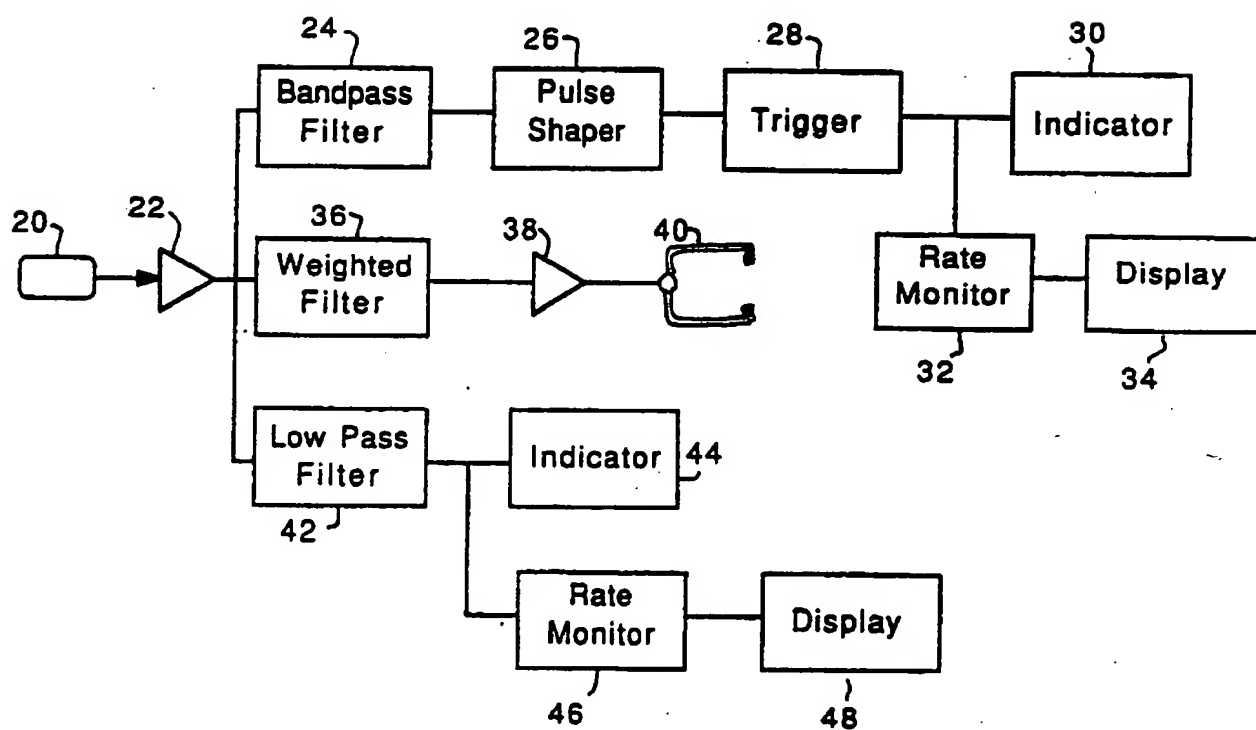
- 2 vibrations comprising a piezoelectric transducer.
- 3 3. The system according to claim 1, said means for detecting said chest wall  
4 vibrations comprising a electromagnetic transducer.
- 5 4. The system according to claim 1, said means for detecting said chest wall  
6 vibrations comprising a resistive transducer.
- 7 5. The system according to claim 1, further comprising means for processing  
8 said output signal to provide an indication of heart sounds produced by said  
9 individual.
- 10 6. The system according to claim 5, further comprising means for using said  
11 heart sounds to calculate the heart rate of said individual.
- 12 7. The system according to claim 6, further comprising a weighted bandpass  
13 filter for processing said output signal, said weighted bandpass filter having  
14 a transfer function equivalent to that of a stethoscope to provide an electrical  
15 signal representation of audible heart sounds, and an audio signal transducer  
16 to convert said electrical representation into an audible heart sound.

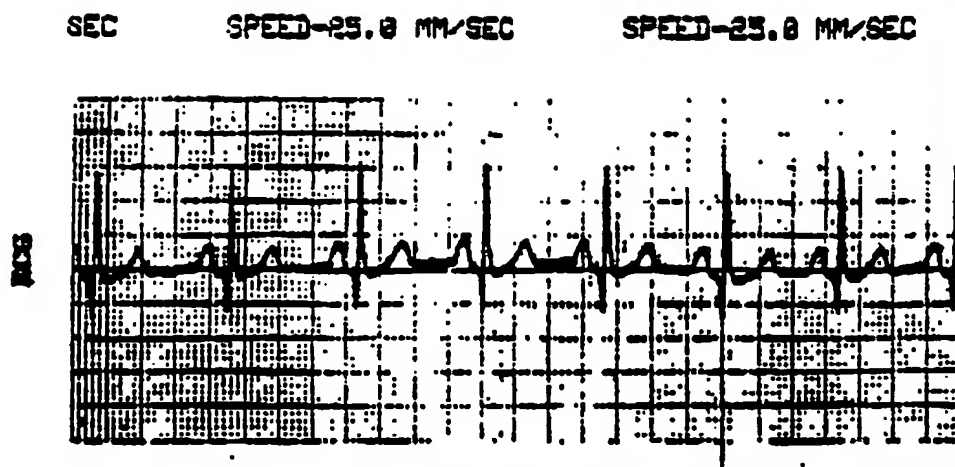
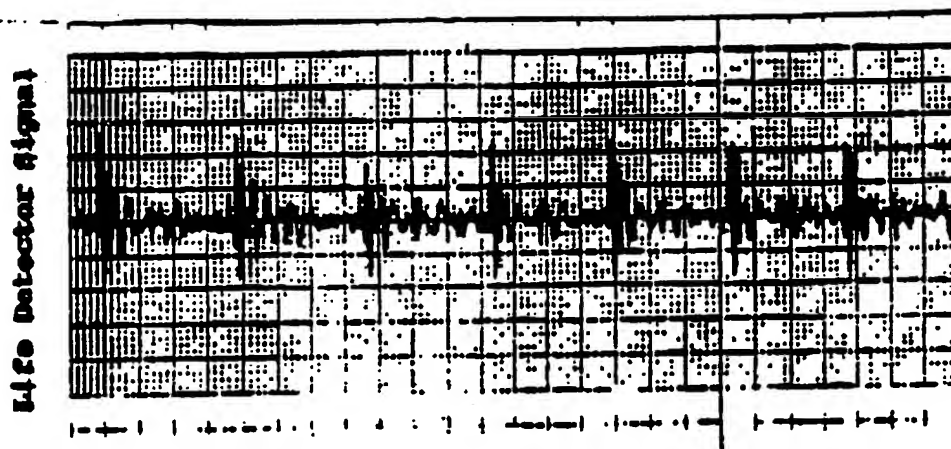
2           said output signal to determine the existence of respiration in said individual.

3           9.     The system according to claim 8, further comprising means for calculating  
4           the respiration rate of said individual.

5           10.    The system according to claim 1, said system being contained in a housing  
6           having sufficient mass to maintain said detector in an effectively stationary  
7           position relative to the body of said individual.

2       A vital life sign detector which can be used to determine heart and respiration activity  
3       in an individual wearing bulky clothing, such as chemical warfare protective clothing.  
4       A detector, such as an accelerometer or geophone, detects chest wall vibrations of an  
5       individual and produces an output signal in response thereto. The output signal is  
6       processed to determine the existence of cardiac and respiratory activity. The output signal  
7       can be further processed to calculate the heart rate and respiration rate of the individual.  
8       The system produces a visual or audio signal which allows medical personnel to  
9       determine quickly whether the individual is alive.

**FIG. 1****FIG. 2**

FIG. 3aFIG. 3b



# INTERNATIONAL SEARCH REPORT

International Application No.

PCT/US91/08905

International Application No. <b>PCI/US91/08905</b>	
<b>I. CLASSIFICATION OF SUBJECT MATTER</b> (If several classification symbols apply, indicate all) <sup>1</sup> According to International Patent Classification (IPC) or to both National Classification and IPC <b>IPC(5): A61B 5/0255</b> <b>US CL 128/715</b>	
<b>II. FIELDS SEARCHED</b>	
Minimum Documentation Searched <sup>2</sup>	
Classification System	Classification Symbols
<b>US</b>	<b>128/715</b>
Documentation Searched other than Minimum Documentation to the extent that such Documents are included in the Fields Searched <sup>3</sup>	
<b>III. DOCUMENTS CONSIDERED TO BE RELEVANT <sup>4</sup></b>	
Category <sup>5</sup>	Citation of Document, " with indication, where appropriate, of the relevant passages <sup>6</sup>
	Relevant to Claim No. <sup>7</sup>
<b>X, Y</b>	<b>US, A, 5,002,060 (NEDIVI) 26 MARCH 1991</b> <b>See entire document.</b>
<b>Y</b>	<b>US, A, 4,840,183 (TAKAHASHI) 20 JUNE 1989</b> <b>See entire document.</b>
<b>Y, P</b>	<b>US, A, 5,010,890 (PFOHL) 30 APRIL 1991</b> <b>See entire document.</b>
<b>A, P</b>	<b>US, A, 4,972,841 (IGUCHI) 27 NOVEMBER 1990</b> <b>See abstract.</b>
<b>A, P</b>	<b>US, A, 5,025,809 (JOHNSON) 25 JUNE 1991</b> <b>See abstract.</b>
<b>* Special categories of cited documents: <sup>8</sup></b> <b>"A"</b> document defining the general state of the art which is not considered to be of particular relevance <b>"E"</b> earlier document but published on or after the international filing date <b>"L"</b> document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified) <b>"O"</b> document referring to an oral disclosure, use, exhibition or other means <b>"P"</b> document published prior to the international filing date but later than the priority date claimed <b>"T"</b> later document published after the international filing date or priority date and not in conflict with the application but cited to underline the grounds or theory underlying the invention <b>"X"</b> document of particular relevance: the claimed invention cannot be considered novel or cannot be considered to involve an inventive step <b>"Y"</b> document of particular relevance: the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art. <b>"A"</b> document member of the same patent family	
<b>IV. CERTIFICATION</b>	
Date of the Actual Completion of the International Search	Date of Mailing of this International Search Report
<b>30 JANUARY 1992</b>	<b>02 MAR 1992</b>
International Searching Authority	Signature of Authorized Officer
<b>ISA/US</b>	<b>NGUYEN NGOC-HO</b>
	<b>SCOTT GETZOW</b>

Form PCT/BA/010 (REVISED 08/00) (Page 11) of 17

DC 2/21/92